Identification of target areas for deep brain stimulation in human basal ganglia substructures based on median nerve sensory evoked potential criteria

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Objectives: In the interventional treatment of movement disorders, the thalamic ventral intermediate nucleus (VIM) and the subthalamic nucleus (STN) are the most relevant electrode targets for deep brain stimulation (DBS). This study tested the value of somatosensory evoked potentials (SEP) for the functional identification of VIM and STN.

Methods: Median nerve SEP were recorded from the final stimulation electrodes targeted at STN and VIM. Throughout the stereotactic procedure SEP were recorded during short electrode stops above STN/VIM and within the presumed target areas. After digital filtering, high and low frequency SEP components were analysed separately to parameterise both the 1000 Hz SEP burst and low frequency (<100 Hz) components.

Results: SEP recorded in the VIM target region could unequivocally be distinguished from SEP recorded in STN. The 1000 Hz burst signal was significantly larger in VIM than in STN without any overlap of amplitude values. In the low frequency band, a primary high amplitude negativity was obtained in VIM, contrasting with a low amplitude positivity in STN. SEP waveforms in recordings above target positions resembled SEP obtained in STN. When entering VIM, a sharp amplitude increase was observed over a few millimetres only.

Conclusions: Based on SEP criteria, the VIM target but not the STN region can be identified by typical SEP configuration changes, when penetrating the target zone. The approach is independent of the patient’s cooperation and vigilance and therefore feasible in general anaesthesia. It provides an easy, reliable, and robust tool for the final assessment of electrode positions at the last instance during electrode implantation when eventual electrode revisions can easily be performed.

Abbreviations: VIM, ventral intermediate nucleus; STN, subthalamic nucleus; DBS, deep brain stimulation; SEP, sensory evoked potential
that SEP were collected during the study but not used for targeting. Criteria were developed in a post hoc analysis of the data obtained.

The electrode model (Medtronic 3389) used consists of a shaft with four ring contacts with a width of 1.5 mm, each, spaced at distances of 0.5 mm. The three basal contacts (anodes) were referenced against the cranial one (cathode), resulting in three bipolar derivations over 4.5 mm, 2.5 mm, and 0.5 mm. In a fourth channel, the compound action potential was derived mediolaterally at the ipsilateral upper arm proving the constancy of nerval input throughout all recording steps.

The median nerve contralateral to the DBS electrode was stimulated at an intensity of twice motor threshold to guarantee saturated responses. Recordings were performed at the end of surgery under intravenous propofol controlled sedation. Electrical stimuli were applied at 8.1 Hz (constant current squarewave pulses of 0.1 ms width) and averaged over 1000 single sweeps. A wide bandpass (5 Hz–1500 Hz) was used for data acquisition (sampling rate 10 kHz). Offline digital high- and lowpass filters (corner frequency: 428 Hz; 24 dB/octave) were applied to separate high frequency from low frequency responses, which, therefore, could be analysed independently.

Amplitudes of the low frequency subcortical (P16) and cortical (N20) SEP components were determined baseline to peak in the 5 Hz–428 Hz bandpass. The duration and amplitude of the high frequency burst component, superimposed to the primary subcortical component and oscillating around 1000 Hz for about 5 ms–10 ms, was determined in the 428 Hz–1500 Hz bandpass. Statistical analyses were performed using two sided paired t tests. Results were considered statistically significant at p levels <0.01.

Electrode positions were determined in a three dimensional system, based on intraoperative radiographs with ventriculography. The anatomical coordinates refer to the position of the second but lowest electrode along the x axis (laterality), describing the lateral distance from ac-pc midline (line between anterior and posterior commissure), along the y axis (anteriority), defined as the sagittal distance from pc (posterior commissure), and along the z axis (depth), defined as the vertical distance from ac-pc (negative values indicating below ac-pc/positive values indicating above ac-pc).

RESULTS

SEP in the VIM region (n=10 of 10 subjects)

SEP recorded from planned VIM targets displayed a specific configuration, distinguishable from SEP waveforms obtained at any other recording site (fig 1). In the low frequency band (<100 Hz) the response is characterised by a single monophasic negative component, sharply rising to an amplitude of 6.9 (5.4) µV (mean (SD)) with a peak latency of 17.3 (2.2) ms. In the high frequency band the 1000 Hz burst signal exhibited an average rms amplitude of 0.43 (0.11) µV, with signal onset at 13.4 (1.2) ms and offset at 22.8 (1.6) ms.

The average coordinates for the VIM target were x=11.6 (2.2) mm, y=6.6 (1.5) mm, and z=-1.8 (1) mm. The z value indicates comparatively low positions. Electrodes targeted to VIM may therefore partially lap into the caudally bordering structure—that is, Zona incerta.

The clinical DBS efficiency was reflected by a decrease of the total tremor score (from 61 (19.1) preoperatively to 24 (18.8) postoperatively; p=5.7×10^(-5)).
SEP in the STN region (n=16 of 11 subjects)
Low frequency SEP, recorded from planned STN targets, are dominated by a positivity of 1.1 (0.4) μV peaking at 18.7 (1.4) ms. The 1000 Hz burst has an amplitude of 0.09 (0.02) μV with an onset at 14.2 (1.3) ms and an offset at 22.6 (1.6) ms (fig 1).

The coordinates of the STN targeted electrodes were x=11 (1.4) mm, y=11.1 (1.7) mm, and z=-2.2 (1.6) mm.

The clinical DBS efficiency was reflected by a reduction on the UPDRS motor scale (37.75 (17.43) preoperatively to 19.1 (16) postoperatively; \( p=4.6 \times 10^{-3} \)).

SEP along the trajectory to VIM (n=14 of 7 subjects) and STN (n=32 of 11 subjects)
SEP recorded 1 cm and 2 cm above STN and VIM hardly differed from those obtained in STN. They were characterised by a primary, monophasic positive potential of comparatively low amplitude. When stepping down from 2 cm to 1 cm above either target position, an increase in amplitude goes in parallel with a decrease in latency. 1 cm and 2 cm above VIM the positive potentials peak at 18.7 (1.9) and 19 (2) ms with amplitudes of 2.4 (1.5) and 1.4 (1) μV, respectively. For the STN trajectory the values are: 19.1 (1.6) and 19.8 (1.6) ms with amplitudes of 1.1 (0.6) and 0.8 (0.2) μV4—that is, a consistent increase in amplitude cannot be seen towards the target zone. Burst signals are of lower amplitude than in the according target regions, most strikingly in the transition to VIM. The rms amplitudes for high frequency SEP 1 and 2 cm above VIM are 0.12 (0.03) and 0.04 (0.02) μV, above STN 0.06 (0.05), and 0.03 (0.01) μV, respectively (fig 1).

Comparison of VIM SEP and STN SEP
The SEP amplitudes of low and high frequency responses were significantly different in STN compared with VIM (low frequency responses: \( p=1.2 \times 10^{-7} \); burst responses: \( p=2.06 \times 10^{-10} \)). All low frequency SEP had negative polarity in VIM and positive polarity in STN. High frequency amplitudes did not overlap between targets. Burst responses recorded in VIM are about four times larger than 1 cm above it, and low frequency components always reverse polarity over this distance. For these low frequency responses, the voltage gradients along the four contact electrode shaft were calculated between electrode contacts 1–4 (used for normalisation), contacts 1–3, and 1–2. These gradients were found to differ significantly (\( p<0.01 \)) between VIM (1: 0.29 : 0.03) and STN (1 : 0.78 : 0.37). Latencies for both components did not differ significantly between the targets.

An interindividually consistent location difference of electrodes was found only for the y coordinate (4.5 mm; \( p=1.03 \times 10^{-6} \)).

Casual observations
Early in the series in two subjects, exhibiting no or minor clinical gains, SEP did not meet the target criteria described above. Instead, sequences of a negative-positive-negative complex with intermediate amplitudes were recorded (see fig 2); this could be correlated to electrode positions between the mean VIM and STN y coordinates in these patients.

In two further patients with planned STN implantations a second surgical intervention was performed for unilateral electrode revisions because of missing clinical stimulation effects. Their SEP configuration resembled a VIM pattern with a monophasic negative component. In both patients the electrodes were shifted to a more anterior position by 3 mm. Correspondingly, after this correction an STN-like SEP configuration was obtained; clinically, both patients improved.

In one subject an additional recording was performed only 3 mm above the target position in VIM: this SEP contained a
low frequency positivity with the typical waveform of trac-torial SEP described above. Driving down the electrode 3 mm into the presumed VIM area, a monophasic negative low frequency response and a high amplitude burst component (15.5 µV; burst: 0.51 µV) were obtained (fig 3).

DISCUSSION

SEP recorded from the definite electrode implant for DBS are reliably indicative for the region targeted for in tremor conditions—that is, VIM/Zona incerta. Parameters of low frequency components and the analysis of recently described local high frequency SEP activity provide useful information for the functional identification of target zones.19 This SEP approach is robust against surrounding electromagnetical noise and provides data independent from the patient’s vigilance level and cooperation.20

The distinct VIM pattern in SEP recordings can be related to the anatomical difference along the γ axis. SEP can thus enrich stereotactic surgery by functional data (fig 2).

Low frequency SEP (<100 Hz)

In routine SEP diagnostics, latency and amplitude of low frequency components (for example, N20 in median nerve SEP) are evaluated in a large variety of neurological disorders to assess the integrity of the somatosensory system. They are assumed to reflect mainly postsynaptic potentials.20,21

When recording from VIM electrodes, a large monophasic negativity peaking around 17 ms was obtained, rapidly decreasing just millimetres above VIM as well as more rostrally towards STN. Given the macroscopic nature of the used electrode, we propose this sharply rising component to originate as mixed near-field contributions from the main somatosensory thalamic relay nucleus (VC), dorsally bordering to VIM (see fig 2), and the caudal VIM itself, which also receives short latency somatosensory input.22 This assumption is based on the following arguments: (1) the rising SEP amplitude gradient, the closer one records to the neighbouring VC/VIM areas, (2) the phase reversal, occurring on the caudal level of VC/VIM, congruent with earlier semi-microelectrode recordings,22 proving short latency somatosensory input as to VIM as to VC, and (3) the steep voltage gradients along the four contact electrode. These findings congruently suggest a near-field origin of the negative wave. Notably, we observed no correlation between SEP recorded in VIM and parasthesias elicited by DBS.

An intermediate SEP configuration was observed casually along a presumed transition zone between VIM and STN. These SEPs are characterised by a diphasic, primarily negative component.

A monophasic positive SEP component of comparatively small amplitude is typically recorded in STN. This configuration was found at all studied recording sites with the exception of recordings near or in VIM. Thus, the low amplitude profile of SEP recorded along STN trajectories makes the search for SEP peak amplitudes for STN targets a useless enterprise.

High frequency SEP (around 1000 Hz)

This burst response of 5–10 oscillatory potentials features fast dynamic characteristics suggesting a generation via synchronised action potentials, eventually from local bursting relay or interneurons and/or the most cranial parts of medial lemniscal fibres.20,21

The analysis of this high frequency response has proved a further useful parameter to identify VIM, but only in cases with comparatively low amplitude low frequency SEP. The burst power was severalfold higher in VIM than in surrounding basal ganglia motor structures, including STN, without any overlap. The steep burst increase, moving from any extrathalamic recording site into VIM, hints at a near field generated potential, probably originating from the neighbouring thalamic relay nucleus.22,23

Comparison with previous SEP studies

In contrast with earlier studies on human subcortical SEP, using cephalic or extracephalic skin reference electrodes, intracranial bipolar recordings were analysed in this study.19,20,24–28 This technical difference could explain the earlier findings of similar SEP patterns in STN and VIM, distinguishable only from SEP recorded in the somatosensory relay nucleus, whereas with the present bipolar montage a polarity change of primary SEP components could be revealed between VIM and more rostral as well as cranial sites.

Only few data have been published on subcortical high frequency SEP bursts, interpreting them as sequential action potentials, arising in the brain stem, medial lemniscus, and thalamus.29 A recent study, using the present bipolar depth recording technique provided support for the hypothesis that the 1000 Hz burst reflects local rather than propagated activity,23 as the narrow bipolar montage (see fig 2) could emphasise near field, high frequency potentials.

Conclusions

SEP from the final electrode for DBS are a useful tool to provide the therapeutic team with functionally based information on the electrode position. The method is capable of supporting VIM target identification for DBS tremor suppression. Occasionally, it provides a clue for corrections in STN surgery in cases of posterior electrode mislocalisations. SEP are recorded at the last instance when corrections can be achieved without a second surgical approach. The method is appealing for its low demands on equipment and its robustness against electromagnetically noisy surroundings. All SEP evaluation criteria are independent from the patient’s vigilance state and cooperation.20 SEP from the definite deep brain electrode do not reach the spatial significance of single cell microrecordings, yet they provide a quick and robust information on the momentary electrode placement. Thus, their position in the diagnostic procedure during DBS implantation, in particular the relation between macroscopic SEP and cellular microelectrode recordings, may be worth further study.

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REFERENCES


NEURONLINE

MS society websites: www.mssociety.org.uk and www.nationalmssociety.org

Patients turning up with folders full of printouts from the internet are increasingly common sights in out-patient departments. The response from clinicians often tends towards annoyance and even suspicion. Furthermore, a disease such as multiple sclerosis is linked to much mystery (concerning causes) and controversy (concerning treatments), and as such, the internet abounds with sites making all manner of claims. Physicians therefore need to be able to recommend informative and reliable sites to patients.

The MS Society (UK) provides an easy-to-use and comprehensive web site (www.mssociety.org.uk). Particularly note worthy are downloadable booklets and information sheets. “Newly-diagnosed” patients are sure to find many of these highly useful. Other sections in the web site include links to local support groups, information on working with MS, insurance issues, and pages for carers. The site also gives an overview of research activity in an accessible and balanced way.

Equally impressive is the US equivalent (www.nationalmssociety.org). Again, information is laid out in a user-friendly way with a multitude of links to other web sites pertaining to the disease. Of particular note to the neurologist, however, is the section on clinical study measures, which sets out in detail, with downloadable forms and user guides, the wide variety of rating scales that have been used in clinical studies of MS, providing a useful resource for all those involved in the management of the disease.

The internet has revolutionised so much of the way we all live our lives, and patients with neurological diseases are increasingly turning to it for information. Control and regulation of information on the internet is a problem, but perhaps if neurologists were to become more involved in writing patient group websites, we could enhance the service we give to patients and prevent some of the more ludicrous medical claims coming to the attention of our patients.

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