Electrophysiological study after surgical repair of sectioned human peripheral nerves

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SUMMARY Clinical and electrophysiological assessment of recovery of function are reported on 20 patients with median or ulnar nerve sections up to 53 months after surgical repair. Maximum improvement of sensory function was apparent by both methods of assessment at 15 months after suture, and thereafter conduction velocities in sensory fibres averaged 80% of normal in median nerves and 70% of normal in ulnar nerves. Similarly, the mean amplitude of the sensory action potential at the wrist remained depressed at 15% of control values. The clinical recovery of motor function pursued a similar time course with, however, some evidence to indicate a continuing improvement in the neurophysiological maturation of the motor nerve fibres up to 47 months after repair. The results are discussed in relation to previous electrophysiological studies on animals.

The recovery of function after traumatic peripheral nerve injury has been assessed clinically both in civilian practice (Nicholson and Seddon, 1957; Edshage, 1968) and in the war-injured (Seddon, 1954). Little information is, however, available concerning neurophysiological details of recovery or how these might correlate with the clinical findings. While there is also a considerable literature based on animal experimentation with a variety of peripheral nerve injuries (Berry et al., 1944; Guth, 1956; Cragg and Thomas, 1964; Jacobson and Guth, 1965; Grabb, 1968), there remains a relative lack of information on the electrophysiological maturation of sectioned and resutured regenerating nerve fibres in humans.

The present investigation was planned to measure the degree of recovery in regenerated human nerves after traumatic section and surgical repair. Quantitative electrophysiological studies of motor and sensory conduction and of the recovery of nerve action potentials have been performed on the median and ulnar nerves in twenty subjects.

METHODS

The fastest motor conduction velocity in the median and ulnar nerves was measured using standard techniques with recording of the evoked motor response in the abductor pollicis brevis or hypothenar muscles respectively (Hodes et al., 1948). For the determination of terminal motor latency, the stimulating electrodes were placed distal to the site of the nerve lesions.

Sensory nerves were studied both orthodromically and antidromically. Orthodromic studies were made by surface stimulation of the digital nerves using silver strip ring electrodes (Dawson, 1956). The thumb, index, and middle fingers were studied in the case of the median nerve, and the little finger for the ulnar nerve. The sensory nerve action potentials (SNAP) were recorded from 0.5 cm diameter saline-padded silver electrodes situated 3 cm apart over the nerve at the wrist with the stigmatic electrode below the site of the lesion. A rectangular electrical stimulus 0.1 msec in duration and two to three times the threshold voltage was used. Antidromic studies were made simply by reversing the sites of stimulation and recording using the same electrodes. In these studies, stimuli were supramaximal for the motor response. The mixed nerve action potential (MNAP) evoked by stimulation of the nerve trunk at the wrist was recorded above the elbow using saline-padded silver surface electrodes as above. A similar electrode was used for stimulation, with the cathode distal to the site of the injury. Rectangular stimuli of 0.1 msec duration were delivered by an isolated constant current stimulator (Devices) triggered by an
external time signal (Digitimer). Stimuli were supra-
maximal by 20% for the motor response; larger
stimuli were not used to avoid stimulation of the
nerve trunk proximal to the electrodes, and to reduce
the possibility of concomitant stimulation of
adjacent nerve trunks, especially that of the radial
nerve in the case of sensory studies.

Potentials were amplified by a low noise amplifier,
having a 2–3 μV noise level with a 5 kHz filter, and
displayed on a storage oscilloscope (Tektronix 564),
together with an external time signal on a separate
channel. For the nerve action potential studies
(MNAP and SNAP) the peak to peak amplitude of the
potential and the latency to the onset of the
initial negative response were recorded. The velocity
was calculated over the corresponding distance be-
tween electrodes.

All studies were repeated on the corresponding
nerve of the contralateral normal limb so that each
parameter could be matched with a control value
obtained from the same subject. The results have
been expressed as a percentage of these internal con-
trols. Mean values have been expressed together with
standard errors of the mean. The investigations were

conducted in a thermostatically controlled room and
skin temperatures were recorded with a surface
thermister. Where necessary the temperature was
adjusted to 37 ± 0·1°C with an infra-red lamp.

**PATIENTS** Twenty patients were investigated aged
15 to 53 (30·9 ± 3·0) years. Fourteen patients had
sustained complete section of the median nerve at the
wrist four to 47 (mean 26 ± 4·2) months before.
Eight patients had sustained complete ulnar nerve
section 13 to 53 (31 ± 4·4) months before. All patients
had undergone surgical exploration and repair. In the
median nerve group 12 repairs were by primary and
two by delayed secondary suture, while in the
ulnar group six primary and two secondary sutures
had been performed.

Muscle power in the abductor digiti minimi (ADM)
or abductor pollicis brevis (APB) was graded clinically
0 to 5 according to the MRC scale (Seddon, 1954), while sensory loss was estimated in terms of the
area of loss to pinprick and light touch, and its
intensity noted as mild, moderate, or severe, depend-
ing on the patient’s subjective response. Tests of
two-point discrimination were made with the calipers

<p>| TABLE |
|-----------------|-----------------|-----------------|-----------------|</p>
<table>
<thead>
<tr>
<th><strong>MEAN VALUES ± SEM</strong></th>
<th><strong>Controls</strong></th>
<th><strong>Sutured nerves</strong></th>
<th><strong>t (paired test)</strong></th>
<th><strong>P</strong></th>
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<tr>
<td><strong>Median nerves (14 subjects)</strong></td>
<td></td>
<td></td>
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<tr>
<td>Motor latency</td>
<td>2.90 ± 0.23</td>
<td>4.00 ± 0.33</td>
<td>3.9542</td>
<td>&lt; 0.01</td>
</tr>
<tr>
<td>Motor conduction velocity (elbow to wrist segment) (msec)</td>
<td>56.38 ± 180</td>
<td>56.70 ± 4.14</td>
<td>0.1847</td>
<td>NS</td>
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<tr>
<td>Antidromic sensory conduction velocity:</td>
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<tr>
<td>Thumb–wrist (m/sec)</td>
<td>44.70 ± 1.93</td>
<td>56.70 ± 4.14</td>
<td>0.1847</td>
<td>&lt; 0.02</td>
</tr>
<tr>
<td>Index–wrist (m/sec)</td>
<td>52.85 ± 1.32</td>
<td>40.87 ± 3.21</td>
<td>3.7981</td>
<td>&lt; 0.01</td>
</tr>
<tr>
<td>Middle–wrist (m/sec)</td>
<td>51.09 ± 1.41</td>
<td>42.84 ± 2.30</td>
<td>3.2943</td>
<td>&lt; 0.01</td>
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<td>Orthodromic sensory nerve action potential amplitude:</td>
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<td></td>
<td></td>
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<tr>
<td>Thumb–wrist (μV)</td>
<td>33.5 ± 2.56</td>
<td>3.99 ± 0.86</td>
<td>10.1593</td>
<td>&lt; 0.001</td>
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<tr>
<td>Index–wrist (μV)</td>
<td>18.75 ± 1.74</td>
<td>2.10 ± 0.90</td>
<td>8.3397</td>
<td>&lt; 0.001</td>
</tr>
<tr>
<td>Middle–wrist (μV)</td>
<td>23.31 ± 3.92</td>
<td>2.04 ± 0.86</td>
<td>5.0450</td>
<td>&lt; 0.001</td>
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<tr>
<td>Mixed nerve action potential conduction velocity</td>
<td></td>
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<tr>
<td>(wrist to above elbow) (10 subjects) (m/sec)</td>
<td>63.84 ± 2.45</td>
<td>57.54 ± 2.04</td>
<td>3.1281</td>
<td>&lt; 0.05</td>
</tr>
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<td>Mixed nerve action potential amplitude (wrist to above elbow) (μV)</td>
<td>47.28 ± 7.46</td>
<td>13.86 ± 2.41</td>
<td>5.0291</td>
<td>&lt; 0.01</td>
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<td><strong>Ulnar nerves (8 subjects)</strong></td>
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<tr>
<td>Motor latency</td>
<td>2.44 ± 0.13</td>
<td>3.73 ± 0.24</td>
<td>4.8984</td>
<td>&lt; 0.01</td>
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<tr>
<td>Motor conduction velocity (below elbow to wrist segment) (m/sec)</td>
<td>57.33 ± 2.43</td>
<td>59.36 ± 6.63</td>
<td>0.2885</td>
<td>NS</td>
</tr>
<tr>
<td>Antidromic sensory conduction velocity (wrist to 5th digit) (m/sec)</td>
<td>54.20 ± 2.31</td>
<td>37.6 ± 5.03</td>
<td>4.0079</td>
<td>&lt; 0.01</td>
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<td>Orthodromic sensory nerve action potential amplitude (5th digit) (μV)</td>
<td>12.63 ± 1.93</td>
<td>1.65 ± 0.62</td>
<td>5.3140</td>
<td>&lt; 0.01</td>
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<tr>
<td>Mixed nerve conduction velocity (wrist to below elbow) (6 subjects) (m/sec)</td>
<td>59.97 ± 3.32</td>
<td>60.37 ± 6.65</td>
<td>0.0457</td>
<td>NS</td>
</tr>
<tr>
<td>Mixed nerve action potential amplitude (wrist to below elbow) (μV)</td>
<td>57.00 ± 13.47</td>
<td>22.50 ± 5.45</td>
<td>3.1034</td>
<td>&lt; 0.05</td>
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RESULTS

MOTOR NERVE STUDIES  Distal motor latencies
(Table, Fig. 1) In the case of two patients examined four and six months after median nerve lesions, no muscle response in the hand could be obtained to indirect stimulation of the nerve. The latencies in patients at 10 to 20 months after median nerve injury remained in excess of normal, decreasing from 233% to 118% of control values over this period, while even after 40 months only two of five patients had a distal latency equivalent to control values. A progressive decrease in the ulnar distal motor latencies was found from a high of 204% at 13 months to a low of 115% at 36 months, but nevertheless normal values were not found even at 53 months.

Conduction velocity in the fastest motor fibres
(Table, Fig. 1) The forearm conduction velocity could first be measured at 10 months and thereafter the values obtained were comparable with those of the controls. Abnormally fast conduction proximal to the site of injury was estimated in three patients at 30, 42, and 45 months respectively, probably as a result of technical difficulties in stimulating the nerve at the site of injury or due to aberrant innervation from cross-anastomosis between the ulnar and median nerves.

CLINICAL ASSESSMENT OF POWER (Fig. 2) In only two of the median nerve group, at 42 and 47

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FIG. 1. (a) Peripheral motor latencies as percentage of control values. (b) Fastest motor conduction velocities as percentage of control. ● Median nerves. X Ulnar nerves.
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months, was power in the APB thought to be in the normal range (grade 5). After 30 months two patients had obtained only grade 3 power or less, while, conversely, four patients studied between 10 and 15 months after injury had regained power of grade 4-4+. In the patients with ulnar nerve lesions, power in the ADM muscle remained subnormal in all patients, grade 4 being the best obtained.

SENSORY STUDIES Median nerve sensory conduction velocities (Table, Fig. 3) We were unable to demonstrate a sensory response to stimulation before 10 months in any digit, while at 10 months a small antidromic response only was obtained from the thumb and middle fingers alone of one patient. The conduction velocities in the regenerated fibres lie mainly between 60 and 95% (mean 80·8 ± 2·9%) of controls, with little evidence that further improvement occurred with the passage of time. The antidromic method was adopted for the assessment of sensory conduction velocity, since a potential could often be detected by this technique when no recordable response to orthodromic sensory stimulation was obtained. In all patients the antidromically-evoked action potential (SNAP) was of shorter latency than the muscle response. However, since the deflection due to the onset of the muscle action potential at times occurred within the duration of the SNAP, only SNAP amplitudes were considered in the statistical analysis. These values have been used for the purpose of estimating the number of regenerated large diameter myelinated fibres. In these studies (Table, Fig. 4), a SNAP was not obtained before a lapse of 10 months, but later studies gave values up to 30% of control amplitude with no tendency to larger potentials with prolonged follow-up. Only three patients had a median SNAP above 30% of control value in a single digit each. There was no

Fig. 2. Clinical assessment of power. (Top) Muscle power (MRC grading). (Bottom) TPD objective sensory testing. Score as percentage control side: • APB. X ADM.
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FIG. 3. Antidromic sensory conduction velocities as percentage of control values. • Thumb. ○ Index finger. □ Middle finger. ✗ Fifth finger.

FIG. 4. Orthodromic sensory action potential amplitudes as percentage of control values. • Thumb. ○ Index finger. □ Middle finger. ✗ Fifth finger.
consistent trend for a better recovery in one digit rather than another.

**Ulnar nerves** Six of the eight subjects had sensory conduction velocities below 70% of normal (mean 67.5 ± 8.5%) with no consistent improvement in the values over the 53 months. The amplitudes of orthodromically evoked SNAP were below 40% in all patients, and in three patients at 30, 36, and 42 months were still unobtainable.

**CLINICAL ASSESSMENT OF SENSORY FUNCTION** (Fig. 2) All patients complained of a sensory deficit to pinprick and cotton wool which varied from mild to severe, but no further attempt was made to quantitate this aspect of sensory loss more accurately. However, since two-point discrimination (TPD) is a more accurate method of quantitating sensory loss in peripheral nerve lesions (Seddon, 1954), this objective assessment was used. The correct scores out of five attempts for each digit have been expressed as a percentage of the control hand; in the case of the median nerve results from thumb, index, and middle fingers were pooled. In the median nerve territory it is apparent that, apart from a severe loss of TPD below 10 months, the score thereafter remains below 70% of normal and does not improve over subsequent months. In the ulnar nerve territory there may be some improvement with the passage of time, but the value still did not exceed 50% of the control.

**EVOKED MIXED NERVE ACTION POTENTIALS** (Fig. 5) The conduction velocity in the median nerve showed a moderate reduction compared with the control values (91 ± 2.6%). There was no tendency to significant improvement with the passage of time. The values in the ulnar nerves were comparable with those of the controls. In contradistinction to the sensory studies, the amplitude of the mixed NAP showed a progressive rise over the period of follow-up. This was more apparent in the median nerve group, where a value of 87% of normal was reached by 47 months. The change was less distinct in the recovering ulnar nerves where one exceptional.

![Figure 5](http://jnnp.bmj.com/)

**FIG. 5.** (a) Evoked nerve action potential conduction velocity as percentage of control side. (b) Evoked mixed nerve action potential amplitudes as percentage of control side. ○ Median. × Ulnar.
high value (122%) linked with a low normal response distorts the results.

**DISCUSSION**

Nicholson and Seddon (1957), in a report of their extensive experience of the results of surgical repair of the median and ulnar nerves in civil practice, found that good recovery of power (grade 4 or better on the MRC scale) had occurred in approximately 30% of subjects by three years. The recovery had been progressive over this period, and further but much slower improvement was present up to five years after suture. The recovery of sensory function followed a similar pattern. We have not found this pattern of recovery in our patients, where a plateau of improvement in power and sensation (as measured with two-point discrimination) was found by 15 months after injury, with no subsequent improvement of note. In the additional light of our electrophysiological studies we feel that a full clinical assessment of recovery from nerve injury at the wrist can be made by 15 to 18 months. While the numbers in the present study are small, we found no indication that age or method of surgical repair (primary or secondary suture) was of importance in the eventual outcome. This is in agreement with Nicholson and Seddon (1957).

Terminal motor conduction, as measured by distal motor latency to nerve stimulation, is determined by the conduction in the largest motor fibres and the delay at the neuromuscular junction. Impairment in either or both of these parameters may be responsible for the distal delay in conduction in regenerating nerves. Berry et al. (1944), in studies on cats after nerve section and suture, found progressive recovery of conduction velocity with time, corresponding to progressive increase in fibre diameters, but at 466 days the fastest conduction velocity remained at only 80% of normal. Hodes and others (1948) similarly found reduced conduction velocity at 60% of normal after regeneration in humans. Cragg and Thomas (1964), in studies of regeneration after crush injury to the peroneal nerve of the rabbit, found that the conduction velocity distal to the site of injury was only 75% of that in the contralateral control nerve at 12 months, and showed no further improvement in animals at 16 months after injury. The largest fibre diameters of the regenerated nerves were similar at both 12 and 16 months, at nearly 90% normal, but the internodal length of the regenerated nerves was less than 50% of control values for the corresponding fibre diameters. They estimated that the myelin thickness in relation to axon diameter was very nearly normal by 16 months. However, Schröder (1972) in morphological studies on dogs of sciatic nerve regeneration after suture and nerve grafting, found that, whereas the mean diameter of regenerated axons reached 79% of normal by 12 months, that of the myelin sheaths was only 57%. No further significant increase in the average maximum fibre diameter or in the thickness of the myelin sheath occurred between 12 and 24 months after grafting. This striking reduction of the thickness of the myelin sheath was present on the largest regenerated nerve fibres as well as the latter being reduced from normal diameter. Rushton (1951) had calculated on theoretical grounds that a decrease in the thickness of the myelin sheath would reduce conduction velocity to a greater extent than a similar decrease in the axon diameter. Hence Schröder suggested that the reduced conduction in regenerated nerve fibres was mainly due to the decreased thickness of the myelin sheath. Defects in neuromuscular transmission have also been reported after human nerve regeneration (Hodes, 1948) and intermittent failure of transmission in experimental regeneration was found by Dennis and Miledi (1971). It thus appears that several factors may play a part in the incomplete motor recovery, as shown by the prolonged distal motor latency in our studies, but we have no information of the effect of repetitive nerve stimulation in our patients.

The mean sensory conduction velocity in the regenerated nerves of this study was 80% of normal in the median nerve and 70% in the ulnar, comparing closely with values of 80% by Berry et al. (1944), and 75% obtained by Cragg and Thomas (1964). Furthermore, the velocity in our studies showed no significant improvement after 10 months from the time of suture. The fastest motor conduction velocities of the main nerve trunks were all within the normal range, indicating no block in conduction at the level of the lesion and no gross slowing over the small segment of regenerating fibres. Unusually fast
conduction was estimated in two median nerves compared with controls, but this was almost certainly due either to branching between the main motor nerves in the forearm or incomplete stimulation of the distal motor fibres within the scar tissue. The fastest velocity in the combined motor and sensory fibres, as measured in the MNAP studies, was similarly close to normal, but surprisingly a progressive increase in the amplitude of the response was found.

In a normal nerve, the amplitude of the evoked action potential is an indication of the number and size of the nerve fibres (Jacobson and Guth, 1965). In a regenerated nerve, the full normal fibre diameters are not attained, and the distribution of fibre size after experimental nerve section and suture remains defective (Gutmann and Sanders, 1943; Cragg and Thomas, 1964). However, in the absence of marked slowing of conduction and temporal dispersion of the NAP, the amplitude of the response evoked by stimulation of the regenerated nerve segment is an index of the number of functional regenerated fibres. The sensory nerve action potentials were all significantly reduced in amplitude and were mainly below 40% of the contralateral control values, with an overall mean of 15% after 15 months. These results compare with the 20% of normal values found by Jacobson and Guth (1965) in the sciatic nerves of the rat. The mixed nerve action potentials, although less reliable because of possible stimulation of proximal nerve fibre stumps at the wrist, similarly showed a reduced amplitude response at a mean of 42 ± 8% of normal after 12 months. In contrast with the SNAP studies, however, there was evidence of a progressive increase in the MNAP amplitude with time. We are uncertain of the explanation for this finding in view of the absence of such a change in the sensory nerves alone. The terminal motor fibres did, however, show a progressive maturation with a progressive decrease in the distal motor latency, and we assume that the sequential improvement in the amplitude of the MNAP must be related to this. Also, narrowing of nerve fibres for a distance proximal to a chronic constrictive lesion has been reported in animals (Anderson et al., 1970). The slow recovery of the mixed NAP may be related to recovery in these fibres and subsequent synchronization of the evoked responses. However, it would appear that with sensory reinnervation after nerve section and regeneration there is a permanent reduction both in the number of functional large diameter fibres and in the fibre diameter. The maximum recovery in nerve lesions at the wrist occurred by 15 months, and we were unable to detect electrophysiological evidence of sensory recovery in the digits before 10 months after injury. This interval is comparable with findings in the radial nerve in which Downie and Scott (1964) were unable to detect a sensory response 6 to 11 months after a traumatic lesion in continuity. A corollary of these findings is that where there is total absence of electrophysiological evidence of nerve regeneration with traumatic lesions of nerves at the wrist by 12 to 15 months, the site of the lesion should be explored and nerve grafting considered.

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REFERENCES


