

Somatosensory evoked potentials following stimulation of the lower limb in cortical reflex myoclonus

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SUMMARY Generating mechanisms of giant somatosensory evoked potentials (SEPs) following stimulation of the posterior tibial nerve as well as the big toe were investigated in three patients with cortical reflex myoclonus. Scalp distributions of recognisable components were very similar to those in normal subjects, except that their amplitude was much larger. The tibial nerve SEPs were remarkably attenuated by interfering tactile stimulation. Therefore, the giant SEPs observed in the present cases seem to be, at least partially, due to input from cutaneous nerve fibres on the background of extremely enhanced excitability in area 3b of the primary sensory cortex where normal SEPs are generated

Somatosensory evoked potentials (SEPs) in patients with "cortical reflex myoclonus"¹ or "pyramidal myoclonus"² are of remarkably high amplitude, and hence they have been commonly called "giant SEPs". Although there have been a number of reports concerning the giant SEPs following stimulation of the upper limbs,^{3–17} no systematic study of SEPs following stimulation of the lower limbs in cortical reflex myoclonus has been reported.

The present study, therefore, aimed at elucidating the pathophysiology of SEPs following stimulation of the lower limbs in cortical reflex myoclonus using various methods such as conventional nerve trunk stimulation, electrical finger stimulation, and the interference approach.^{18–22} In particular, the detailed scalp topography of each component was investigated.

Patients and methods

Three patients were carefully selected from those who manifested myoclonus, according to the following criteria: (1) the amplitude of the initial cortical positive potential recorded at or around the somatosensory leg area of the scalp following stimulation of the posterior tibial nerve at

the ankle was larger than the mean plus 2 standard deviations of normal subjects, (2) enhanced long-loop reflex (C reflex, termed by Sutton and Mayer⁷) could be recorded even at rest (without voluntary contraction of the corresponding muscle), and (3) the presence of cortical spike was demonstrated by the jerk-locked averaging method^{9 14 23} to precede a spontaneous myoclonic jerk.

All patients manifested intention as well as postural myoclonus, and they were taking normal doses of anti-myoclonus medication, as listed in table 1, to suppress myoclonus at the time of study. SEPs following stimulation of the upper limbs in all three cases were also of remarkably high amplitude.

Recordings were performed in a quiet, dimly lit room. The patient was kept awake in a reclining arm-chair, and was encouraged to relax. The electrical stimulus was a constant voltage square-wave pulse of 0.2 ms duration. It was delivered to the right posterior tibial nerve at the ankle. The stimulus intensity was sufficient to produce a definite twitch of the big toe. The right big toe was stimulated using silver ring electrodes with the stimulus intensity approximately 15 mA.

Interfering tactile stimulus was applied by the experimenter by gently rubbing the right sole using a soft wad of tissue paper continuously and concurrently with the electrical stimulation of the posterior tibial nerve.

Silver disc recording electrodes were attached at 19 scalp locations based on the international 10–20 system. LFC, MFC, RFC, LCP, MCP and RCP electrodes were midway between corresponding sites of the 10–20 system as indicated in fig 1. All sites were referred to the linked earlobes (A1A2). The frequency response of the amplifiers was between 1 and 1500 Hz (–3dB). Five hundred responses to the posterior tibial nerve stimulation and 1000 responses to the big toe stimulation were averaged. At least three recordings were

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Table 1 Patients with cortical reflex myoclonus subjected to the present study

Case	1	2	3
Diagnosis	Progressive myoclonic epilepsy	Sialidosis type 2	Uremic encephalopathy
Sex and age	Female, 17 yr	Male, 55 yr	Female, 15 yr
Other symptoms	Cerebellar ataxia	Cerebellar ataxia	Consciousness disturbance
Medication at the time of study	Clonazepam 6 mg Valproate 800 mg Primidone 500 mg	Clonazepam 4 mg Valproate 600 mg Propranolol 60 mg	Phenytoin 200 mg

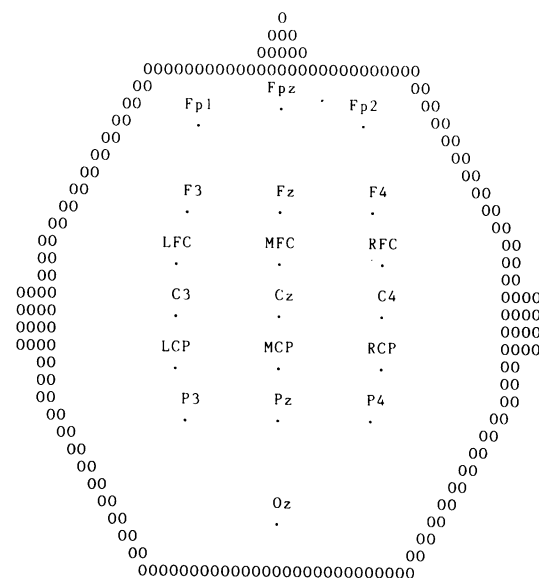


Fig 1 Electrode placements based on the international 10-20 system. LFC, MFC, RFC, LCP, MCP and RCP were midway between F3 and C3, Fz and Cz, F4 and C4, C3 and P3, Cz and Pz, and C4 and P4, respectively. The linked earlobes (A1 + A2) were used as the reference.

made for each stimulus condition. An analysis window was 5-125 ms for the posterior tibial nerve stimulation and 10-130 ms for the big toe stimulation. The sampling rate was 0.23 ms. Responses contaminated with large artifact over 200 μ V were rejected by a computer program.

Table 2 The amplitude of recognisable components in normal subjects as well as in patients with cortical reflex myoclonus in the present study

Stimulus site	Electrode	Component	Amplitude (μ V)			
			Control (n = 18) mean \pm SD	Case 1	2	3
Posterior tibial nerve at ankle	MCP	P39	1.6 \pm 0.7	5.1	6.5	10.0
	F3	N39	1.0 \pm 0.4	1.8	2.7	2.5
	MCP	N48	3.5 \pm 1.4	15.6	9.7	10.5
Big toe	F3	P48	1.5 \pm 0.7	8.8	5.0	6.0
	MCP	P39	0.7 \pm 0.3	4.1	1.8	2.2
	F3	N39	0.3 \pm 0.2	1.0	1.0	0.7
	MCP	N48	1.7 \pm 0.8	6.4	4.0	5.5
	F3	P48	0.7 \pm 0.3	2.5	1.6	2.2

Each recognisable component was cursorred for the peak latency and amplitude, the latter being measured from the preceding peak of the opposite polarity. The upper limit of the normal range was set to the mean plus 2 SD of the value obtained from 18 normal subjects in our department for each recording session (table 2).

Scalp topography of each consistent component was drawn using two different methods. In the first method, the topography was drawn using the peak-to-peak amplitude of each peak visually identified by the experimenter at each electrode to show its scalp distribution. The second method, which was the so-called isopotential map, was based on the amplitude from the baseline at each electrode at a particular time interval after the stimulus onset. The baseline was determined by averaging the deflection of the first 10 ms of the analysis window at each electrode.

Relative positivity at grid 1 resulted in a downward deflection in all recordings. Each recognisable component was named, because of the similarity of its wave form to that of the normal SEPs, according to the previous report of normal SEPs,²¹ and it was based on the polarity and peak latency.

Results

(1) SEPs following stimulation of the posterior tibial nerve at ankle

The wave forms recorded at the MCP and F3 electrode in the present cases as well as in one normal subject, whose data were selected as a representative in terms of the wave form and the scalp topography, are shown in fig 2. The amplitude of P39 and N48 at the MCP electrode was much larger than the normal range in all three cases (table 2 and fig 2). N33 was identified before P39 in all three cases, but its ampli-

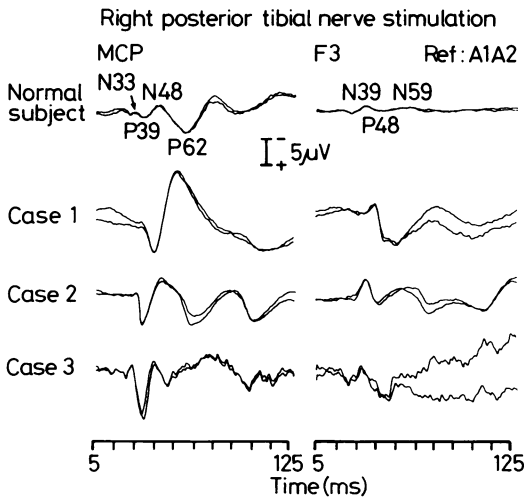


Fig 2 Wave forms of SEPs following stimulation of the right posterior tibial nerve at ankle recorded at two selected electrodes in one normal subject to show the nomenclature of each recognisable component, and in the present three cases. N33 is not so large in each case. In contrast, P39 and N48 at the MCP as well as N39 and P48 at the F3 electrode are very large in the present cases.

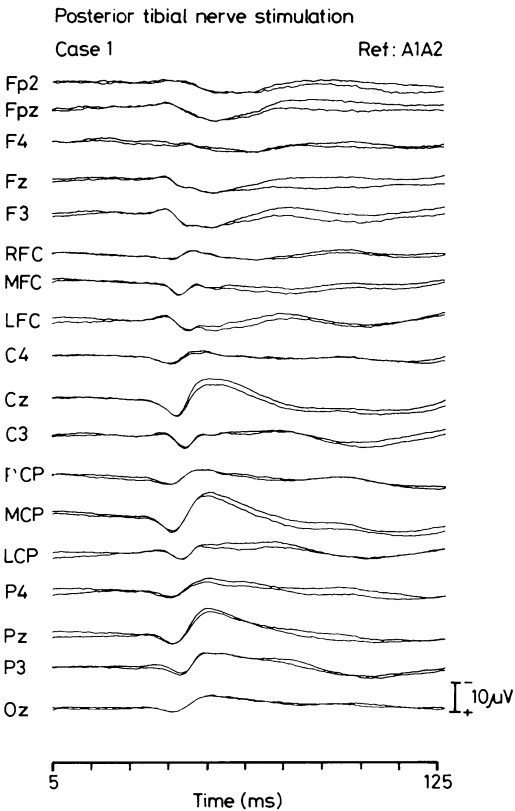


Fig 3 Wave forms of SEPs at all electrodes following stimulation of the right posterior tibial nerve at ankle in case 1. 500 responses were averaged.

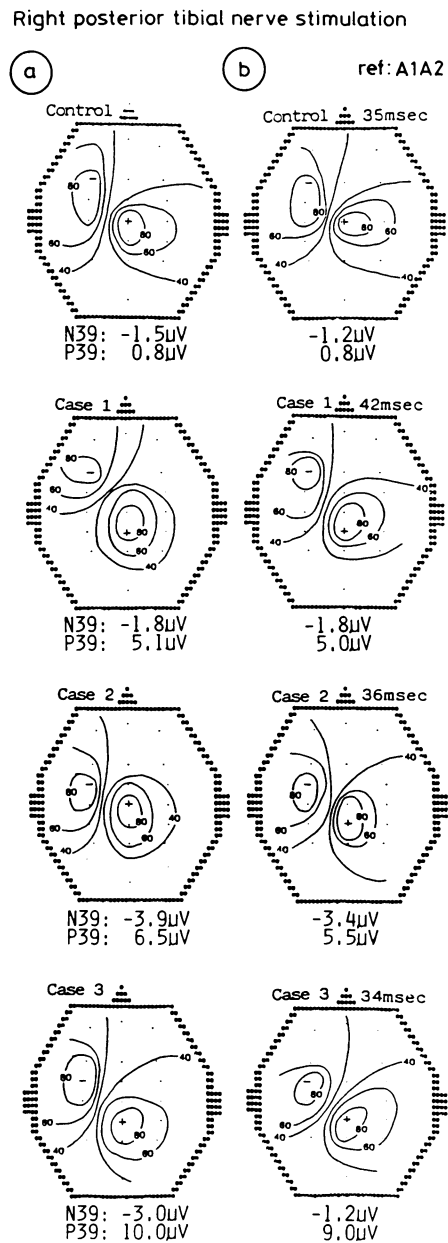


Fig 4 Scalp topography of P39-N39 complex in one normal subject as well as in each individual case. In (a), it was drawn using the peak-to-peak amplitude to show the distribution of P39 and N39, and in (b), it was drawn using the amplitude measured from the baseline at the latency when P39 was maximal in each individual record (isopotential maps). Electrode marked - or + shows the maximal point of the negative and positive component, respectively, and its amplitude is shown below each figure. 80, 60 and 40 are the percentage amplitude with respect to the maximal point. P39 is maximal at the Cz or MCP electrode, and N39 is maximal at the F3 or LFC electrode in the normal subject as well as the present cases.

Right posterior tibial nerve stimulation

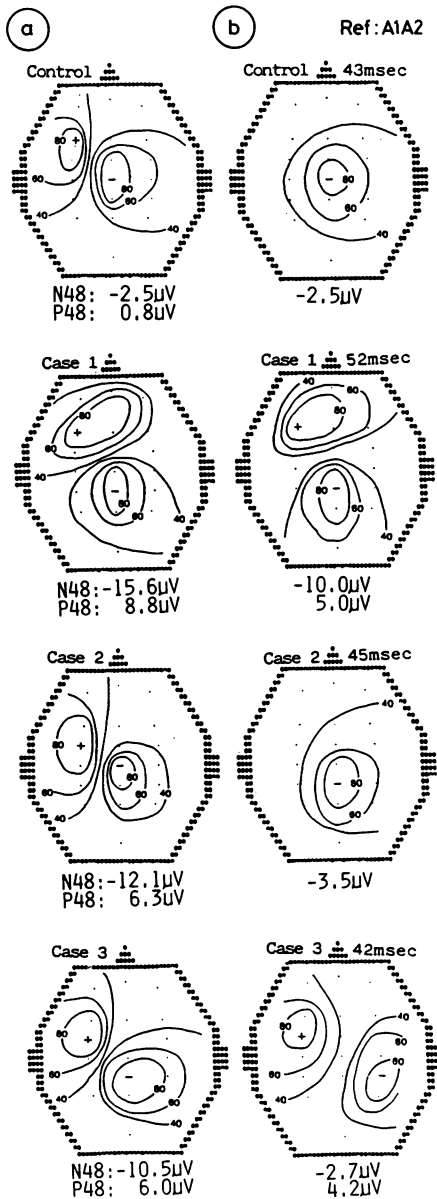


Fig 5 Scalp topography of N48-P48 complex based on the peak-to-peak amplitude (a), and isopotential maps at the latency when N48 was maximal in each individual record (b). (refer to the legend for fig 4). In (a), N48 is maximal at the Cz or MCP electrode, and P48 is maximal at the F3 or LFC electrode in the normal subject as well as the present cases. However, the isopotential maps in (b) are relatively different from those in (a) probably because of the influence of the preceding P39 and N39 components.

tude was within the normal range. The amplitude of N39 and P48 at the F3 electrode was also larger than the normal range, but was relatively smaller compared with P39 and N48 (table 2 and fig 2). The wave forms of components following N48 and P48 were variable from case to case. SEPs at all electrodes in case 1 were shown in fig 3.

The peak latencies of P39, N39, N48 and P48 were within the normal range. The peak latencies of P39 and N48 at the MCP electrode showed no significant difference from those of N39 and P48 at the F3 electrode, respectively (paired *t* test.).

Scalp distributions of P39-N39 and N48-P48 complexes in each case as well as in one normal subject were shown in figs 4A and 5A, respectively. In all three cases, both P39 and N48 potentials were maximal at the MCP or Cz electrode, and spread in the central and parietal regions more to the hemisphere ipsilateral to the stimulated nerve. N39 and P48 were maximal at the F3 or LFC electrode, and spread to the frontal and central regions over the hemisphere contralateral to the stimulated nerve. Isopotential maps at the latency when P39 was maximal (fig 4b) were very similar to the scalp distribution of the P39-N39 complex (fig 4a), but those at the latency when N48 was maximal appeared different from the scalp distribution of N48-P48 complex in case 2 and normal subject (fig 5), probably because of the influence of the preceding P39 and N39. The scalp distributions of those components in three cases were almost the same as those of our normal subjects as well as those from the previous reports,^{21 24} in terms of the maximal point and distribution of each component, and of the orientation as well as the bordering area of their scalp distributions.

(2) Interfering effects

Interference effects by the continuous tactile stimulation applied to the sole ipsilateral to the stimulated nerve are shown at two selected electrodes, F3 and MCP (table 3 and fig 6). P39 and N48 at the MCP

Table 3 Amplitude changes of SEPs following stimulation of the right posterior tibial nerve at ankle due to concurrent interfering tactile stimulation of the right sole

Electrode	Component	Control*	Case		
			1	2	3
MCP	P39	-34%	-59%	-27%	-62%
F3	N39	-21%	-56%	-46%	-16%
MCP	N48	-33%	-60%	-29%	-33%
F3	P48	-27%	-61%	-47%	-14%
F3	N59	-10%	-69%	-20%	+18%
MCP	P62	-15%	-58%	-3%	-29%

*The average change due to interference in 18 normal subjects

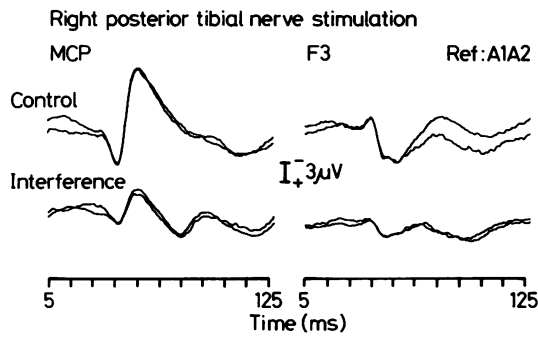


Fig 6 Wave form changes of SEPs at two selected electrodes following stimulation of the right posterior tibial nerve at ankle by concurrent tactile stimulation applied to the right sole in case 1. The upper traces are conventional SEPs (Control) and the lower ones are SEPs with interference (Interference). 500 responses were averaged. Each potential at each electrode is markedly attenuated by the tactile interference.

electrode were remarkably reduced in cases 1 and 3, and moderately reduced in case 2. N39 and P48 at the F3 electrode were moderately reduced in cases 1 and 2, and slightly reduced in case 3. In contrast, the changes of the following components, N59 and P62, varied from subject to subject. Compared with the interference effects in normal subjects, the relative changes were consistently larger in case 1, but were not different in cases 2 and 3 (table 3).

(3) SEPs following stimulation of the big toe
The wave forms of SEPs following electrical stimulation of the big toe by using ring electrodes (fig 7) were almost the same as those following the posterior

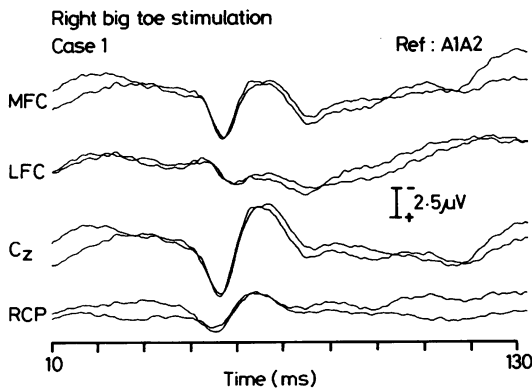


Fig 7 Wave forms of SEPs at four selected electrodes following stimulation of the right big toe in case 1. 500 responses were averaged. The potentials, corresponding to P39, N39 and the following potentials to posterior tibial nerve stimulation, are also very large.

tibial nerve stimulation. The amplitude was smaller than that to the posterior tibial nerve stimulation, but was much larger than the normal range in all cases (table 2). The scalp topographies of recognisable components were not significantly different from those of the corresponding components following stimulation of the posterior tibial nerve.

Discussion

To our knowledge, this is the first systematic study of SEPs following stimulation of the lower limb in cortical reflex myoclonus. P39, N39, N48 and P48 are considered to be cortical potentials like those in normal subjects,^{21 24-30} since they showed a clearly localised distribution. Scalp distributions of P39 and N48 (figs 4 and 5) suggest that their generator source might be the leg region of the primary sensory cortex. Not only P39 and N48 recorded in the parietal region but also N39 and P48 recorded in the contralateral frontal region were larger than the normal range, and they were similarly reduced by tactile stimulation. Moreover, the difference of peak latencies between P39 and N39, or between N48 and P48 was not statistically significant. Therefore, it seems reasonable to consider that frontal potentials, N39 and P48, result from an orientation of dipolar activities generated in the primary sensory cortex, as reported in the studies of normal subjects.^{21 25 27 30}

The components following stimulation of the big toe, corresponding to P39-N39 and N48-P48 of the tibial nerve SEPs, were also very large in each case, and their scalp distributions were very similar to those of the corresponding potentials following stimulation of the posterior tibial nerve. Moreover, the P39-N39 as well as N48-P48 complexes of the tibial nerve SEPs were considerably attenuated by tactile stimulation applied to the sole ipsilateral to the stimulated nerve in each case (fig 6 and table 3). These findings suggest that those potentials following the posterior tibial nerve stimulation might be, at least partially, due to input from cutaneous nerve fibres. This is compatible with the study of normal subjects in our previous report.²¹ Therefore, the generator source for giant P39-N39 and N48-P48 complexes may contain, as for SEPs in normal subjects,²¹ area 3b in the primary sensory cortex whose neurons receive input mainly from cutaneous nerve fibres.³¹

In conclusion, it seems reasonable to consider that giant SEPs following stimulation of the lower limb in cortical reflex myoclonus are generated by the same mechanisms as SEPs in normal subjects, although the excitability of the generator source, probably area 3b, must be extremely enhanced. This conclusion is not different from that for generating mechanisms of giant SEPs following stimulation of the upper limb in

our previous report.¹⁷ In that study,¹⁷ N19 and P19, corresponding to the so-called N20 and P20, were not enlarged, but the following potentials, both P25 in the contralateral parietal region and N25 in the frontal region, were of remarkably large amplitude. Therefore, it seems reasonable to consider that the small negative deflection, N33 recorded at the parietal electrodes following the posterior tibial nerve stimulation, corresponds to N20 of the median nerve SEPs, and that the following potentials, P39 and N39, correspond to P25 and N25 of the median nerve SEPs, respectively.

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References

- Hallett M, Chadwick D, Marsden CD. Cortical reflex myoclonus. *Neurology* 1979;29:1107-25.
- Halliday AM. The electrophysiological study of myoclonus in man. *Brain* 1967;90:241-84.
- Dawson GD. The relation between the electroencephalogram and muscle action potentials in certain convulsive states. *J Neurol Neurosurg Psychiatry* 1946;9:5-22.
- Dawson GD. Investigations on a patient subject to myoclonic seizures after sensory stimulation. *J Neurol Neurosurg Psychiatry* 1947;10:141-62.
- Watson CW, Denny-Brown D. Studies of the mechanism of stimulus-sensitive myoclonus in man. *Electroencephalogr Clin Neurophysiol* 1955;7:341-56.
- Halliday AM, Halliday E. Cortical evoked potentials in patients with benign essential myoclonus and progressive myoclonic epilepsy. *Electroencephalogr Clin Neurophysiol* 1970;29:106-7.
- Sutton GG, Mayer RF. Focal reflex myoclonus. *J Neurol Neurosurg Psychiatry* 1974;37:207-17.
- Chadwick D, Hallett M, Harris R, Jenner P, Reynolds EH, Marsden CD. Cortical, biochemical, and physiological features distinguishing myoclonus responsive to 5-hydroxytryptophan, tryptophan with a monoamine oxidase inhibitor, and clonazepam. *Brain* 1977;100:455-87.
- Shibasaki H, Yamashita Y, Kuroiwa Y. Electroencephalographic studies of myoclonus: myoclonus-related cortical spikes and high amplitude somatosensory evoked potentials. *Brain* 1978;101:447-60.
- Kelly JJ Jr, Sharbrough FW, Daube JR. A clinical and electrophysiological evaluation of myoclonus. *Neurology* 1981;31:581-9.
- Rothwell JC, Obeso JA, Marsden CD. On the significance of giant somatosensory evoked potentials in cortical myoclonus. *J Neurol Neurosurg Psychiatry* 1984;47:33-42.
- Obeso JA, Rothwell JC, Marsden CD. The spectrum of cortical myoclonus. From focal reflex jerks to spontaneous motor epilepsy. *Brain* 1985;108:193-224.
- Shibasaki H, Neshige R, Hashiba Y. Cortical excitability after myoclonus: jerk-locked somatosensory evoked potentials. *Neurology* 1985;35:36-41.
- Shibasaki H, Yamashita Y, Neshige R, Tobimatsu S, Fukui R. Pathogenesis of giant somatosensory evoked potentials in progressive myoclonic epilepsy. *Brain* 1985;108:225-40.
- Tobimatsu T, Fukui R, Shibasaki H, Kato M, Kuroiwa Y. Electrophysiological studies of myoclonus in sialidosis type 2. *Electroencephalogr Clin Neurophysiol* 1985;60:16-22.
- Cowan JMA, Rothwell JC, Wise RJS, Marsden CD. Electrophysiological and positron emission studies in a patient with cortical myoclonus, epilesia partialis continua and motor epilepsy. *J Neurol Neurosurg Psychiatry* 1986;49:796-807.
- Kakigi R, Shibasaki H. Generator mechanisms of giant somatosensory evoked potentials in cortical reflex myoclonus. *Brain* (in press).
- Jones SJ. An 'interference approach' to the study of somatosensory evoked potentials in man. *Electroencephalogr Clin Neurophysiol* 1981;52:517-30.
- Jones SJ, Power CN. Scalp topography of human somatosensory evoked potentials: the effect of interfering tactile stimulation applied to the hand. *Electroencephalogr Clin Neurophysiol* 1984;58:25-36.
- Kakigi R, Jones SJ. Effect on median nerve SEPs of tactile stimulation applied to adjacent and remote areas of the body surface. *Electroencephalogr Clin Neurophysiol* 1985;62:252-65.
- Kakigi R, Jones SJ. Influence of concurrent tactile stimulation on somatosensory evoked potentials following posterior tibial nerve stimulation in man. *Electroencephalogr Clin Neurophysiol* 1986;65:118-29.
- Kakigi R. Ipsilateral and contralateral SEP components following median nerve stimulation: effects of interfering stimuli applied to the contralateral hand. *Electroencephalogr Clin Neurophysiol* 1986;64:246-59.
- Shibasaki H, Kuroiwa Y. Electroencephalographic correlates of myoclonus. *Electroencephalogr Clin Neurophysiol* 1975;39:455-63.
- Desmedt JE, Bourguet M. Color imaging of parietal and frontal somatosensory potentials fields evoked by stimulation of median or posterior tibial nerve in man. *Electroencephalogr Clin Neurophysiol* 1985;62:1-17.
- Cruse R, Klem G, Lesser RP, Lueders H. Paradoxical lateralisation of cortical potentials evoked by stimulation of posterior tibial nerve. *Arch Neurol* 1982;39:222-5.
- Kakigi R, Shibasaki H, Hashizume A, Kuroiwa Y. Short latency somatosensory evoked spinal and scalp-recorded potentials following posterior tibial nerve stimulation in man. *Electroencephalogr Clin Neurophysiol* 1982;53:602-11.
- Seyal M, Emerson RG, Pedley TA. Spinal and early scalp-recorded components of somatosensory evoked potentials following stimulation of the posterior tibial nerve. *Electroencephalogr Clin Neurophysiol* 1983;55:320-30.
- Kakigi R, Shibasaki H. Scalp topography of the short latency somatosensory evoked potentials following posterior tibial nerve stimulation in man. *Electroencephalogr Clin Neurophysiol* 1983;56:430-7.
- Kakigi R, Shibasaki H, Hashizume A, Shima F, Kuroiwa Y. Short latency somatosensory evoked spinal, thalamic and scalp-recorded potentials following posterior tibial nerve stimulation in man. In: Homma S, Tamaki T, ed. *Fundamentals and Clinical Application of Spinal Cord Monitoring*. Tokyo: Saikon Press, 1984:345-60.
- Kakigi R, Shibasaki H. The effect of aging on somatosensory evoked potentials following stimulation of the posterior tibial nerve in man. *Electroencephalogr Clin Neurophysiol* 1987;68:277-86.
- Paul RL, Merzenich M, Goodman H. Representation of slowly and rapidly adapting cutaneous mechanoreceptors of the hand in Brodmann's area 3 and 1 of *Macaca mulatta*. *Brain Res* 1972;36:229-49.