RESEARCH PAPER

NMDA receptor binding in focal epilepsies

C J McGinnity,1,2,3 M J Koepp,4,5 A Hammers,1,2,3,4,5,6 D A Riaño Barros,1,2 R M Pressler,7 S Luthra,8 P A Jones,8 W Trigg,8 C Micallef,9 M R Symms,4,5 D J Brooks,1,10 J S Duncan4,5

ABSTRACT
Objective To demonstrate altered N-methyl-D-aspartate (NMDA) receptor availability in patients with focal epilepsies using positron emission tomography (PET) and [18F]GE-179, a ligand that selectively binds to the open NMDA receptor ion channel, which is thought to be overactive in epilepsy.

Methods Eleven patients (median age 33 years, 6 males) with known frequent interictal epileptiform discharges had an [18F]GE-179 PET scan, in a cross-sectional study. MRI showed a focal lesion but discordant EEG changes in two, was non-localising with multifocal EEG abnormalities in two, and was normal in the remaining seven patients who all had multifocal EEG changes. Individual patient [18F]GE-179 volume-of-distribution (Vt) images were compared between individual patients and a group of 10 healthy controls (47 years, 7 males) using Statistical Parametric Mapping.

Results Individual analyses revealed a single cluster of focal Vt increase in four patients; one with a single and one with multifocal MRI lesions, and two with normal MRIs. Post hoc analysis revealed that, relative to controls, patients not taking antidepressants had globally increased [18F]GE-179 Vt (+28%; p<0.002), and the three patients taking an antidepressant drug had globally reduced [18F]GE-179 Vt (−29%; p<0.002). There were no focal abnormalities common to the epilepsy group.

Conclusions In patients with focal epilepsies, we detected primarily global increases of [18F]GE-179 Vt consistent with increased NMDA channel activation, but reduced availability in those taking antidepressant drugs, consistent with a possible mode of action of this class of drugs. [18F]GE-179 PET showed focal accentuations of NMDA binding in 4 out of 11 patients, with difficult to localise and treat focal epilepsy.

INTRODUCTION
N-methyl-D-aspartate (NMDA) receptors are ligand-gated and voltage-gated ion channels that mediate fast excitatory neurotransmission in the central nervous system (CNS).1,2 NMDA receptor-mediated neurotransmission is necessary for cognition, memory and neuronal survival, but excessive NMDA receptor activation mediates excitotoxic neuronal injury following acute cerebral insults,3 is associated with cell death4 and is thought to contribute to disorders of neuronal hyperexcitability, such as epilepsy and neuropsychiatric pain, and chronic neurodegenerative diseases,5 depression6 7 and schizophrenia.8 In chemical models, administration of agonists of either the NMDA or α-amino-3-hydroxy-5-methyl-4-isoxazolepropionic acid (AMPA)/kainate receptors induces convulsions in vivo either by directly mediating an epileptic depolarisation through the NMDA calcium channels or by indirectly activating NMDA channels subsequent to AMPA/kainate receptor activation9 10 (for review: ref. 12). Blockade of NMDA receptors is neuroprotective,13 prevents paroxysmal depolarisation shifts, which are the intracellular correlate of interictal epileptiform discharges (IEDs),14–17 and blocks the development of kindling.18–20 Several21 22 but not all kindling model studies have shown the presence of increased NMDA receptor availability in the hippocampus and cerebral cortex of epileptic animals. Autoradiography of human epileptogenic temporal lobe tissue has revealed increased NMDA receptor availability in the parahippocampal gyrus, in contrast to decreased availability in the hippocampi, particularly in sclerotic regions.23 24 In vitro studies in tissue resected from patients with epilepsy have associated NMDA receptor-mediated neurotransmission with epileptic activity.25–30 Receptor activation, however, can only be shown in vivo. Human microdialysis studies have revealed marked elevations in extracellular glutamate concentration preceding and during seizures,31–37 which would be expected to result in increased NMDA receptor activation. Hence, there is interest in the development of radioligands that allow assessment of NMDA receptor function in humans in vivo.

We have previously observed good brain penetration, moderately heterogeneous distribution in grey matter and suitable rapid washout of the novel NMDA positron emission tomography (PET) tracer [18F]GE-179 in healthy controls.38 This ligand binds at the phencyclidine (PCP) recognition site39 within the NMDA ion channel pore, and hence requires receptor activation for access. This ‘pore-blocker’ ligand could potentially allow use-dependent imaging of the NMDA receptor in the active/open state using PET. We report the first use of [18F]GE-179 PET in focal epilepsies of different focal and multifocal onset. The objective of this proof-of-principle study was to demonstrate in vivo a hypothesised increased NMDA receptor activation in patients with drug-resistant epilepsy.

METHODS
The study was approved by the Research Ethics Committees of the Royal Marsden Hospital, Imperial College Healthcare NHS Trust and University College London Hospitals NHS
Epilepsy and control populations
This was a proof-of-principle, cross-sectional pilot study with targets of 12 participants per group. Eleven patients with refractory focal epilepsies (median age 33 years; range 20–50 years; 6 males) were recruited from the outpatient clinics at the National Hospital for Neurology and Neurosurgery. Demographics and clinical details are listed in Table 1. Their diagnoses were based on history, seizure semiology, prolonged and repeated interictal and ictal EEG recordings (where available), and MRI data. Patients were chosen who had frequent interictal spikes on previous EEG recordings, which we hypothesised would maximise our chances to detect increased binding to open NMDA receptors. None of the patients were taking an antiepileptic drug (AED) known to act at the NMDA receptor. Exclusion criteria included inability to provide informed consent, claustrophobia, standard MR contraindications, a positive urinary pregnancy test on the day of the PET scan and history of drug abuse. Patient 4, whose seizures consisted of a sustained fluctuation of perception of brightness with pupillary hippus, has been presented in a detailed case report.30

The control group, 9 of whom have been described previously,38 comprised 10 healthy volunteers without history of neurological or psychiatric illness (median age 46 years; range 25–62 years; 7 males). Additional exclusion criteria were as described for the patients above. A further three seemingly healthy individuals were subsequently excluded; one due to excessive movement throughout the PET scan acquisition, one whose MRI revealed evidence of a cerebral infarct, and one who was discovered to have a history of benzodiazepine abuse. The original control group data were used, rather than repeat images; the patient data were acquired at approximately the same time as those of the control group (i.e. within 12 months) using the same imaging protocol.

Median age and body mass index (BMI) were compared between patients and control groups by Mann-Whitney U statistic in SPSS. Gender balance was compared between groups with the (Pearson) χ2 test.

MRI data acquisition
Three-dimensional volumetric T1-weighted coronal MRI sequences were acquired at Epilepsy Society (Chalfont St. Peter, UK), as previously described.38 MRIs were reviewed by an experienced neuroradiologist (CM). MRIs were not available for one control participant, in whom 3.0 T MRI was contraindicated.

EEG
All patients had an EEG during the PET scan using a Trackit 18/8 (Lifelines Limited, Hants, UK) ambulatory EEG recorder and an ECI E1 Cap (Electro-Cap International, Eaton, Ohio, USA) with 19 electrodes placed according to the International 10–20 system. An additional reference electrode (Fpz) was sited just anterior to Fz. The O1 and O2 electrodes were removed from the cap prior to scanning for several patients in order to minimise discomfort. The participants were closely observed for evidence of seizures throughout the scan. EEGs were reviewed by an experienced clinical neurophysiologist (RMP). The number of IEDs during the first 30 min of scan acquisition was quantified and correlated with [18F]GE-179 global volume-of-distribution (Vf) using Spearman’s r correlation coefficient.

PET image acquisition and data analysis
PET image acquisition has been described previously.38 Briefly, images were acquired using a Siemens/CTI ECAT EXACT3D 962 HR+PET camera (Siemens, Erlangen, Germany) at Hammersmith Imanet Limited. Each participant had a 90 min dynamic emission scan with a smooth bolus intravenous injection of median 187 MBq (range 173–192 MBq) [18F]GE-179 administered 30 seconds after starting image acquisition. For calculation of continuous decay-corrected and metabolite-corrected parent plasma input functions, discrete arterial blood samples were taken throughout the scan, with continuous arterial blood sampling for the first 15 minutes.

The area under the metabolite model curves (AUCmetabs) was used as a measure of the rate of metabolism for each individual. The AUCmetabs over t=0–30 minutes and t=0–90.5 minutes was compared between groups by multivariate general linear model (GLM), with gender as a fixed factor, and age and BMI as covariates. The residual sum of squares (RSSmetabs) for the metabolite model curve was compared between groups by univariate GLM. The threshold for statistical significance was p=0.05.

The Vf of [18F]GE-179 was computed at the voxel level for each participant by exponential spectral analysis, as described previously.38 Each participant’s Vf image was spatially normalised using a scanner-specific template. To enable group-wise comparisons, images acquired from patients with an epileptogenic zone in the right hemisphere (3 patients) were left-right flipped prior to normalisation; three control participants’ images were also left-right flipped prior to group-wise comparison (controls 1, 4 and 6, selected at random). For individual (1 patient vs 10 controls) comparisons, the native (unflipped) patient and control images were used.

The primary outcome measure, global Vf, was computed as an overall mean over the entire matrix, thresholded at 1/8 of that value to create a brain mask, and averaged again within this mask. The global Vf values were compared between groups using an univariate GLM, with gender as a fixed factor, and age and BMI as covariates.

In order to identify changes in the regional distribution of activated NMDA receptors, group-wise SPM8 analyses based on the smoothed (12 mm Full Width at Half Maximum (FWHM) isotropic Gaussian kernel), transformed parametric Vf images, were performed, comparing patients with focal epilepsy against the controls. The images were compared on a voxel-by-voxel basis using a two-sample t test, assuming unequal variances, with global Vf taken into account via an analysis of covariance (ANCOVA) by group. The images were grey and white matter (explicit) masked, with relative threshold masking at 0.4. We report differences in [18F]GE-179 Vf at p<0.001 (uncorrected), clusters at p<0.05 (uncorrected) and an extent threshold of 15 voxels.

In order to identify participant-specific changes in the regional distribution of activated NMDA receptors, individual SPM8 analyses based on the smoothed transformed parametric Vf images were also performed for each of the patients with frequent IEDs against the 10 controls. Equal variances were assumed and global Vf taken into account via an ANCOVA by group. The unflipped Vf image for each control participant was compared with those of the nine other controls in an identical fashion.
<table>
<thead>
<tr>
<th>ID</th>
<th>Age/sex/handedness</th>
<th>Probable localisation MRI/EEG/MEG</th>
<th>Onset/duration (years)</th>
<th>Postictal interval</th>
<th>Treatment</th>
<th>Seizures</th>
<th>EEG</th>
<th>MEG</th>
<th>MRI</th>
<th>[18F]FDG-PET</th>
<th>Global [18F]GE-179 V₁</th>
<th>Approximately N of observed IEDs (t=0–30 min)</th>
<th>[18F]GE-179 V₁ increases</th>
<th>[18F]GE-179 V₁ decreases</th>
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</thead>
<tbody>
<tr>
<td>1</td>
<td>41/M/R</td>
<td>L frontal</td>
<td>14.5/26.5</td>
<td>6.0 h</td>
<td>CBZ, LEV, LTG, ZNS</td>
<td>SPS, CPS, SGS</td>
<td>L frontotemporal</td>
<td>NA</td>
<td>R IFG lesion</td>
<td>L temporal</td>
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<td>62</td>
<td>L frontal</td>
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<tr>
<td>2</td>
<td>22/M/R</td>
<td>L temporal</td>
<td>4/18</td>
<td>7.5 h</td>
<td>CBZ, LEV, LAC</td>
<td>CPS, SGS</td>
<td>L frontotemporal and R temporal</td>
<td>NA</td>
<td>L HS</td>
<td>L temporal</td>
<td>7.20</td>
<td>43</td>
<td></td>
<td></td>
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<td>3</td>
<td>38/M/L</td>
<td>Multifocal MRI, EEG/MEG</td>
<td>2.5/36.5</td>
<td>45 min</td>
<td>CBZ, CLB, PHT, TPM, fexofenadine</td>
<td>SPS, CPS, SGS</td>
<td>R frontotemporal</td>
<td>L front temporal, L and R temporal</td>
<td>Bilateral tubers: F, P, L-O, periventricular calc</td>
<td>Bilateral tubers: L and R frontal, L temporal, R parieto-occipital, L occipital</td>
<td>NA</td>
<td>4.53</td>
<td>EEG data corrupted</td>
<td>Brainstem; L temporal; R temporal</td>
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<td>28/F/R</td>
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<td>10/18</td>
<td>20.5 h</td>
<td>LEV, sertraline, amiodipine</td>
<td>SPS (pulmonary hippocus)</td>
<td>R temporoparietal</td>
<td>R parieto-occipital &gt;L temporal &gt;L occipital</td>
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<td>R parietal</td>
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<td></td>
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<tr>
<td>5</td>
<td>50/F/R</td>
<td>MRI negative Multifocal EEG/MEG</td>
<td>11/39</td>
<td>39 days</td>
<td>LEV, PHT, lofepramine</td>
<td>CPS SGS</td>
<td>L&gt;R temporal</td>
<td>L and R temporal</td>
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<td>L temporal</td>
<td>5.32</td>
<td>26</td>
<td>R frontal</td>
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<td>33/M/L</td>
<td>MRI negative Unifocal EEG/MEG</td>
<td>19/14</td>
<td>NA</td>
<td>CLN, RUF, fluoxetine</td>
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<td>16/7</td>
<td>3 days</td>
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<td>SPS, SGS</td>
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<td>12.5/28</td>
<td>11 days</td>
<td>CLB, LAC, OXC</td>
<td>SGS</td>
<td>L&gt;R frontal</td>
<td>L F</td>
<td>Neg</td>
<td>L frontal</td>
<td>8.40</td>
<td>42</td>
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<tr>
<td>9</td>
<td>24/M/R</td>
<td>MRI negative Multifocal EEG/MEG</td>
<td>7/17</td>
<td>6.5 h</td>
<td>LAC, LEV, LTG, OXC, CLB</td>
<td>SPS, CPS</td>
<td>R frontocentral</td>
<td>L frontal &gt;L insula, &gt;L frontotemporal</td>
<td>Neg</td>
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<tr>
<td>10</td>
<td>50/F/R</td>
<td>MRI negative Multifocal EEG/MEG</td>
<td>13/37</td>
<td>10+years</td>
<td>LEV, LAC, LTG</td>
<td>CPS</td>
<td>L&gt;R temporal</td>
<td>L and R T</td>
<td>Neg</td>
<td>NA</td>
<td>8.17</td>
<td>Cont epileptiform activity*</td>
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<tr>
<td>11</td>
<td>20/F/R</td>
<td>MRI negative Multifocal EEG</td>
<td>14/6</td>
<td>39.5 h</td>
<td>CLB, OXC</td>
<td>CPS, SGS</td>
<td>R&gt;L temporal</td>
<td>NA</td>
<td>Neg</td>
<td>8.88</td>
<td>3</td>
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</tbody>
</table>

Antidepressant drugs (patients 4–6) are displayed in bold font.

*EEG revealed continuous ongoing focal epileptiform activity in patient 10, who had not shown clinically evident seizure activity within the preceding 10 years. Underline indicates concordance between the cluster of increase and the location of the presumed epileptogenic zone, where known.

Calc, calcification; CBZ, carbamazepine; CLB, clobazam; CLN, clonazepam; CPS, complex partial seizures; EEG, electroencephalography; F, frontal lobe; F/M, female/male; [18F]FDG-PET, [18F]fluorodeoxyglucose positron emission tomography; HS, hippocampal sclerosis; ID, identifying number; IED, interictal epileptiform discharges; IFG, inferior frontal gyrus; L/R, left/right; LAC, lacosamide; LEV, levetiracetam; LTG, lamotrigine; MEG, magnetoencephalography; MRI, magnetic resonance imaging; NA, not available; Neg, negative, that is, no significant findings; O, occipital; OX, oxcarbazepine; P, parietal lobe; PHT, phenytoin; RUF, rufinamide; SGS, secondary generalised seizures; SPS, simple partial seizures; TPM, topiramate; VAL, valproate; V₁, volume-of-distribution; ZNS, zonisamide.


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RESULTS
There was no difference between patient and control group in terms of age (p=1.00), BMI (p=1.00) or gender mix (p=0.47).

There were no significant differences in the AUCmetabs or the RSSmetabs between the groups (p=0.19 and p=0.47, respectively). Age, BMI and gender also did not significantly influence the AUCmetabs (all p>0.09).

Global changes in $V_T$
Global $V_T$ was higher in the focal epilepsy group (median 7.51, range 3.77–8.66) than in controls (median 6.21, range 5.37–7.56), although this did not reach statistical significance (p=0.40). There were two distinct subgroups of patients with higher (n=8) and lower (n=3) than normal global $V_T$. To explore this distribution in patients further, post hoc analysis revealed large and significant differences in global $V_T$ between patients with focal epilepsy who were not taking antidepressant drugs (median 7.97, range 6.04–8.66; +28% relative to controls), and those who were taking antidepressant drugs (median 4.40, range 3.77–5.15; −29% relative to controls), and controls (6.21, range 5.37–7.56; all p<0.002; figure 1).

There were no differences (in gender, age, AUCmetabs, RSSmetabs, BMI, number of IEDs in the first 30 min postinjection) to explain the occurrence of high-$V_T$ and low-$V_T$ patients other than their use of antidepressants.

Frequent IEDs were noted in the EEG of eight patients throughout the first 30 min of scan acquisition. Global $V_T$ did not correlate with the frequency of IEDs measured in the first 30 min after radiotracer injection.

In the following analyses, in order to detect focal increases in activated NMDA receptors over and above global increases, the contribution of global $V_T$ to variance was removed by an ANCOVA by group.

Focal changes—group comparisons
There were no common areas of relative focal decrease or focal accentuations of the globally increased $[^{18}F]GE-179$ $V_T$ in the patient group compared with controls.

Relative decreases in $V_T$—individual comparisons
A focal decrease in $[^{18}F]GE-179$ $V_T$ was seen in two healthy control participants (control 3 mid-parietal; control 4 frontal pole). A relative focal decrease in $[^{18}F]GE-179$ VT was seen in two patients (table 2). None of these changes reached significance after correction for multiple comparisons. In one patient (patient 10), the area of relatively decreased $V_T$ was concordant with one of the multiple tubers seen on MRI.

Relative increases in $V_T$—individual comparisons
Focal increases in $[^{18}F]GE-179$ $V_T$ were seen in one control participant (control 4), maximal in the left parieto-occipital region. A focal increase above global baseline increase in $[^{18}F]GE-179$ $V_T$ was seen in four patients (table 3 and figure 2). Where known, the largest cluster was localised to the lobe of the presumed epileptogenic zone in one, as was the second largest cluster of a further two patients.

DISCUSSION
Using $[^{18}F]GE-179$ PET, we identified global increases in NMDA receptor ion channel availability for patients with focal epilepsies who were not taking antidepressants, whereas tracer binding was globally decreased in those patients with epilepsy who were also taking antidepressant drugs. Increases in $[^{18}F]GE-179$ $V_T$ are consistent with an increase in activated/open NMDA receptors in actively discharging cortex as shown in preclinical work.21 22 We suggest that increased NMDA activation in patients with chronic focal epilepsy extends beyond the presumed epileptogenic zone and is a global phenomenon, as reflected in the increased global $V_T$.

Our group analyses did not identify any focal redistribution of activated NMDA receptor availability in this group of heterogeneous patients with focal epilepsies arising from different cortical locations; this is perhaps not surprising given the heterogeneity and small sample size. For this pilot study, patients were selected based on the frequency of IEDs on previous EEGs, to maximise our chances of detecting increases in NMDA binding. Concordance of $[^{18}F]GE-179$ foci with EEG, structural and functional imaging in individual patients is difficult to assess.
given that some of our cohort had normal or EEG-discordant MRI and poorly defined epileptogenic zones: the epileptogenic zone could not be localised using high-resolution MRI, ictal EEG recordings, magnetoencephalography and fluorodeoxyglucose PET (FDG-PET) in four patients, and could only be lateralised to one lobe in four of the remaining seven patients. In contrast, our individual [18F]GE-179 PET analysis identified focal clusters of increased NMDA receptor activation in four patients with focal epilepsy, and these were concordant with the location of the presumed epileptogenic zone in two of those three patients, in whom this could be lateralised to one lobe. Patient 1 was one of the best-localised cases in our cohort, having concordant scalp EEG, [18F]FDG-PET and ictal single-photon emission CT findings. An intracranial EEG recording over the left temporal lobe revealed a diffuse ictal onset, consistent with spread from a nearby lobe. Consistent with these data, a large cluster of increased $V_T$ was observed in the left frontal lobe for this participant.

Interestingly, a focal increase in [18F]GE-179 $V_T$ was seen in the brainstem of the patient with ictal pupillary hippus in addition to left and right temporal lobe increases (patient 4). The patient is now seizure-free after resection of the tumour in the right parieto-occipital region. Our finding suggests the unusual ictal manifestation might result from a broad epileptogenic network that encompassed the brainstem in close proximity to the nuclei of the oculomotor (III) nerve.

The proportion of NMDA receptors that are active in the resting physiological state is unknown, and the power to detect subtle regional changes in channel opening superimposed on global differences in binding, induced by the epileptic brain or reduced by concomitant use of antidepressants, was limited by our small sample size and conservative thresholds. Studies of unequivocally unifocal epilepsies are now needed to determine whether focal increases of [18F]GE-179 binding may be apparent at epileptic foci. If these initial findings are replicated, [18F]GE-179 PET might find clinical application in the presurgical localisation of epileptogenic foci in patients with refractory focal epilepsy with non-contributory MRI.

Interictal regional cerebral blood flow (rCBF) studies usually show reduced perfusion in focal epilepsy,44 and significant increases in rCBF scans were only seen with prolonged discharges of 8–105 seconds after electrostimulation.45 Our findings are unlikely to reflect changes in cerebral blood flow (ie, altered [18F]GE-179 availability) as decreased perfusion in the epileptogenic zone would likely result in decreased [18F]GE-179 availability and thus $V_T$. While NMDA receptor ion channel opening and the excitatory postsynaptic current are extremely rapid events,46,47 grey matter uptake and the metabolism of [18F]GE-179 occurs over minutes.48 Hence, we interpret the $V_T$ data as indicative of the integrated extent of NMDA receptor activation during the tracer uptake phase (first 30 min) of the scan.

The lack of focal increases in $V_T$ for 7 of the 11 patients with focal epilepsy did not appear to relate to the frequency of scalp-detected IEDs. Global [18F]GE-179 $V_T$ was not significantly correlated with the number of IEDs in the first 30 min following injection. The true extent of epileptic activity will not be detectable on scalp EEG, which may explain the lack of correlation between focal spike activity and global [18F]GE-179 uptake. Moreover, it would be oversimplistic to assume a linear relation between global [18F]GE-179 $V_T$ and IED frequency. We expect that NMDA receptors involved in generation of the IED would rapidly internalise45–47 or desensitise following their activation.46–50 Individual short IEDs would be very difficult to visualise over a 90 min PET scan with [18F]GE-179. We assume any observed increase of [18F]GE-179 binding to be related to underlying generalised baseline overactivity, rather than to transient NMDA channel opening over a few milliseconds.

In the only other in vivo PET study of NMDA ion channel activity in epilepsy, Kumlien et al.51 did not detect focal increases in receptor availability using (S)-[N-methyl-11C]ketamine.

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### Table 2

<table>
<thead>
<tr>
<th>Patient ID</th>
<th>Probable localisation (EEG)</th>
<th>MRI</th>
<th>[18F]GE-179 $V_T$ decreases</th>
<th>Cluster size (mm$^3$/voxels)</th>
<th>Peak voxel coordinates (x, y, z; mm)</th>
<th>$Z_{max}$</th>
<th>Cluster level p (uncorrected)</th>
</tr>
</thead>
<tbody>
<tr>
<td>7</td>
<td>R frontal</td>
<td>L temporal</td>
<td>[18F]GE-179 $V_T$</td>
<td>3968/496</td>
<td>58–20–22</td>
<td>4.32</td>
<td>0.003</td>
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</table>

The cluster(s) reaching significance at $p<0.05$ uncorrected are listed. The contribution of global $V_T$ to variance was removed by an ANCOVA by group. ANCOVA, analysis of covariance; EEG, electroencephalography; ID, identifying number; L/R, left/right; mm, millimeters; MRI, magnetic resonance imaging; $V_T$, volume-of-distribution.

### Table 3

<table>
<thead>
<tr>
<th>Patient ID</th>
<th>Probable localisation (EEG)</th>
<th>MRI</th>
<th>[18F]GE-179 $V_T$ increases</th>
<th>Cluster size (mm$^3$/voxels)</th>
<th>Peak voxel coordinates (x, y, z; mm)</th>
<th>$Z_{max}$</th>
<th>Cluster level p (uncorrected)</th>
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</thead>
<tbody>
<tr>
<td>1</td>
<td>L frontotemporal R IFG lesion</td>
<td>R frontal</td>
<td>[18F]GE-179 $V_T$</td>
<td>7000/875</td>
<td>−32 234</td>
<td>4.46</td>
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<td>4</td>
<td>Multifocal</td>
<td>Brainstem</td>
<td>[18F]GE-179 $V_T$</td>
<td>5152/644</td>
<td>06–28–38</td>
<td>4.58</td>
<td>0.001</td>
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</table>

The cluster(s) reaching significance at $p<0.05$ uncorrected are listed. The contribution of global $V_T$ to variance was removed by an ANCOVA by group. Underline indicates concordance between the cluster of increase and the location of the presumed epileptogenic zone, where known.

ANCOVA, analysis of covariance; EEG, electroencephalography; ID, identifying number; IFG, inferior frontal gyrus; L/R, left/right; mm, millimeters; MRI, magnetic resonance imaging; $V_T$, volume-of-distribution.
Interestingly, each participant in that temporal lobe epilepsy (TLE) cohort showed temporal hypometabolism on $[^{18}F]$ FDG-PET, so the results could have been significantly confounded by cerebral hypoperfusion. Four of our patients had normal $[^{18}F]$FDG-PET, one of whom had a focal increase in $[^{18}F]$GE-179 $V_T$. The absence of hypometabolism may have facilitated visualisation of activated NMDA receptors in our cohort. Alternatively, our cohort might have had more actively spiking cortex, and thus possibly greater NMDA receptor activation.

A striking and unanticipated finding of our study was reduced $V_T$ in the small number of patients with focal epilepsies who were taking antidepressants, suggesting that either depression or the use of antidepressant drug constituted an additional confounder. Our finding is in keeping with the mounting evidence for the action of antidepressant drugs at NMDA receptors including tricyclics$^{52–56}$ and serotonin-selective reuptake inhibitors$^{54 55 57 58}$ such as fluoxetine,$^{57 59–61}$ the two classes used by patients in this study. While our finding may represent the first in vivo evidence of an NMDA-mediated mechanism of action of antidepressants (the extent of which is likely to vary between drugs), caution is warranted as, given the sample size, the result could be due to random chance. Hence, in order to better understand $[^{18}F]$GE-179 binding, a larger study is required, which would compare $[^{18}F]$GE-179 binding between unmedicated patients with depression and those taking antidepressants. It will also be of interest to ascertain whether AEDs that are characterised by use-dependent inhibition of NMDA receptor function (such as felbamate$^{52, 61}$), or certain combinations of AEDs, affect NMDA receptor binding.

A recent multicentre review concluded that administration of the NMDA receptor antagonist ketamine ‘likely’ or ‘possibly’ contributed to the achievement of control in 32% of (19 of 60) episodes, whereas treatment was discontinued due to adverse events in approximately 8%.$^{66}$ Smaller series have reported greater success.$^{65 66}$ Similarly to $[^{18}F]$GE-179,$^{38}$ ketamine binds to the PCP site in the NMDA ion channel pore.$^{67}$ Hence, the demonstration of increased NMDA receptor activation via $[^{18}F]$GE-179 PET might aid the stratification of patients with refractory status epilepticus.

Limitations of this proof-of-principle study include the small and heterogeneous population. While $[^{18}F]$GE-179 has a low affinity for other CNS receptors in vitro,$^{38}$ we cannot exclude the possibility that non-specific binding confounded the analyses. Further studies are needed to confirm our findings, and to quantify reproducibility and specificity of $[^{18}F]$GE-179 binding in vivo.

In conclusion, our results provide in vivo evidence for widespread increases in activated NMDA receptor availability in patients with focal epilepsies. A PET radioligand that reliably demonstrates focal increases in NMDA receptor activity in humans in vivo would hold potential as a method to investigate epileptogenesis in vivo after brain injury, to investigate the role of activated NMDA receptor availability in other conditions, and possibly in the presurgical investigation of patients with refractory focal epilepsy.

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Epilepsy

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are only available to the investigators at present. Any request for data can be
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Data sharing statement
The authors have submitted all major results from the study for publication. Unpublished data consist of individual imaging data sets and
are only available to the investigators at present. Any request for data can be
addressed to the corresponding author; any data sharing will be subject to
restrictions based on anonymisation rules.

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